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EEG Artifact Removal Strategies for BCI Applications: A Survey

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ABSTRACT:

This paper aims to provide a comprehensive examination of the Brain-Computer Interface and the more scientific discoveries that have resulted from it. The ultimate goal of this review is to provide extensive research in BCI systems while also focusing on artifact removal techniques or methods that have recently been used in BCI and important aspects of BCIs. In its pre-processing, artifact removal methodologies were critical. Furthermore, the review emphasizes the applicability, practical challenges, and outcomes associated with BCI advancements. This has the potential to accelerate future progress in this field. This critical evaluation examines the current state of BCI technology as well as recent advancements. It also identifies various BCI technology application areas. This detailed study shows that, while progress is being made, significant challenges remain for user advancement A comparison of EEG artifact removal methods in BCI was done, and their usefulness in real-world EEG-BCI applications was talked about. Some directions and suggestions for future research in this area were also made based on the results of the review and the existing artifact removal methods.

KEYWORDS: EEG, BCI, ECG, EMG, EOG.

1. INTRODUCTION

1.1. Signal Capturing Block

The electrophysiological signals used by the BCI are captured by the Signal Capturing Module. The brain is the source of these signals [7]. Both invasive and non-invasive methods have been developed for BCI research, but invasive methods like electrocardiograms (ECoG) and single-neuron recordings have proven more effective [7,8]. Comparison of signal quality with other non-invasive brain imaging techniques, including magnetoencephalography, positron emission tomography, functional magnetic resonance imaging, near-infrared spectroscopy, and fMRI [8]. The acquired signals are amplified to increase their strength before transmission. Before any computer application, they must be encoded.

1.2. Signal Capturing Block

As illustrated in Fig. 1, preprocessing of EEG signals is an essential first step in any brain-computer interface-based application. The signal is cleaned up by subtracting out artifacts like ECG, EOG, and EMG measurements, filtering out noise, and resampling it to meet detector input specifications.

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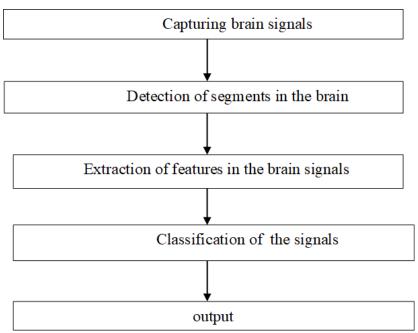


Fig. 1. Stage of the Signal Processing in BCI.

Pre-processing is often done to increase the recorded data's signal to noise ratio before processing. Artifacts in the EEG signal can be eliminated by filtering out the electrical activity produced by head and eye muscle contractions. In order to remove artifacts from an EEG recording, a preprocessing of the signal is required. When properly implemented, BCI systems can Accurate categorization relies heavily on the EEG signal being properly preprocessed. The EEG signal can be cleaned up and made ready for analysis by doing some preliminary processing. BSS, which stands for "blind source separation," is a popular pre-processing method [9]. Artifacts are frequently observed in many forms of EEG signals, as shown in Table 1.

Table 1. Different artifacts arised during signal acquisition of EEG signal processing.

S.No	Artifacts	Artifacts Generated By The Source		Voltage	Shape /Structure	
				Level		
1	Ocular	ar Eye		80-100mv	Delta waves	
	Artifacts (EOG)					
2	EMG	Jaw movements	4-6hz	0-10mv	Theta waves	
3	ECG	Heart or cardiac movement	0-150hz	1-10mv	Beta and gamma waves	
4	50/60 HZ	Power line attached	50/60 hz	high	Beta and gamma	
	artifacts(power				waves	
	line artifacts)					
5	Sweat artifacts	weat artifacts sweat		300 micro	Delta waves	
				volts		
6	Electrode pop	Electrodes attached to scalp	0-30hz	20 mv	Shape appeared	
					different from actual	
					EEG signal	
7	Physical	Body movements,head	Very low	high	Shape appeared	
	movement	movement, jaw movement etc			different from actual	
	artifacts(motion				EEG signal	
	artifacts)					
8	Electronic	Mobile,laptop,personal	Very low	high	Shape appeared	
	gadgets artifacts	computer etc			different from actual	
					EEG signal	

2. LITERATURE REVIEW

The below Table.2 compare the latest artifacts removal techniques in various parameters such as type of artifacts that can able to eliminate in EEG signal processing which is mainly related to BCI applications, novelty in the algorithm or method that chosen to mitigate artifacts, the data that can operated on which the proposed method can best suited (real &simulated) so that we can estimate practical implementation, and also here discussed the challenges or limitations faced to practical viability and commented or given remarks about each and every system of implementation. The above table contain different artifacts removal techniques EOG, ECG, EMG, Physical movement artifacts(motion artifacts) etc but mainly focused on ocular or Eye Blink (EB) artifacts because the EB artifacts are main cause of error or distortion in EEG signal pre-processing.

Table 2. Comparison of various artifacts removal techniques

Table 2. Comparison of various artifacts removal techniques								
Author	Type	Method	Algorithm	Novelty	Data	Challenges/	Comment	
	of artifact		used			limitations	S	
Çınar,	Only	Independent	The classical	The	Real	It is only	The	
Salim(2021)[22	Eye blink	Component	Least Mean	proposed	&simulated	applicable to	proposed	
]	(EOG)	Analysis (ICA),	Squares (LMS)	system does		this method is	method has	
		Kurtosis, K-	and	require an		that ocular	high	
		means, Modified	Normalized	external		artifacts and	performance	
		Z-Score (MZS)	LMS (NLMS)	electrode for		other artifacts	in both	
		and Adaptive		measuring		present it is not	datasets &	
		Noise Canceller		EOG Signals		efficient	comfortable	
		(ANC).				method and	measurement	
		` ′				When	for patients	
						conducting the		
							time EEG	
							recordings.	
						disadvantage is	C	
						the relevant		
						EEG signals		
						can be erased.		
Cao,	Only	Gaussian	cascaded	No false	Real and	-	In terms	
	Eye blink			positives were			of precision	
(2021) [24]	•	(GMM)		found in the	Simulated		and F1 score,	
(2021) [21]	(EGG	(GIVIIVI)	method and the				the proposed	
				eye blink		artifacts caused		
				artifacts using		by eye blinks		
				the suggested		•	reliable.	
				approach.		employing a	i cii de i ci	
				арргоаст.		high threshold.		
Egambaram	Only	FastEMD-	It is	More than	simulate	The	Eyeblink	
Egambaram	Eye blink		proposed to use				artifacts can	
A chycony atal		FastCCA		Accuracy and		EEG samples		
•	(EOG	rasicca		an average of		_	removed	
[26]			Empirical	an average of 10-13ms			online with	
			Decomposition	removal speed			minimal neural	
			and Canonical					
							distortion.	
			Correlation					
			Analysis to					
			perform					
			unsupervised					
			eye blink					
			artifact					
			detection					
-			(eADA).					

Borowicz,	Only	independent	multichann	When	Real and	utilizing	When
			el Wiener filter			C	compared to
7 Kumi. [27]			(MWF) and a		Simulated		the state-of-
	`	and principles of					the-art
				suggested		enhanced off-	
		_		algorithm is			new
				more		implementatio	methodology
				straightforwar		n, and	
				d. Real-time		expanding the	suitable to
				systems can		suggested	real-time
				benefit more			systems.
				from it, and		applicability to	
				that seems to		additional	
				be a crucial		types of	
				factor in BCI		biomedical	
				research and		data.	
				development.			
Zhou,	Only	ICA method	Independen		Real and		This method
	Eye blink			algorithm uses	simulated	1 2	was
Jean Gotman	(EUG		Analysis (ICA) combining			distributions of slow waves and	
[28]			the EEG dipole	computational		visual artifacts	
			model	Without			filter out
			model	requiring		-	EEG
				access to a			aberrations
				database of			attributable
				reference			to the eyes.
				artifacts, it can			,
				separate the			
				EEG from the			
				noise.			
. Sreeja, S.		morphologic		The	Real and	3	
R., et al [29]	y Eye		SVD are two	suggested			applicable to
		analysis (MCA)		sparsity-based			the
			approaches that	* *		necessitates the	
	also used		can be used to	eliminate EB			of other
	for other		eliminate	artifacts in an			artifacts in
	artifacts removal		artifacts.	EEG signal without the use		channels in order to capture	raw EEG
	Temovai			_		ocular artifacts.	uata as well.
				of any specialized		ocuiai aitiiacts.	
				equipment or			
				additional			
				channels for			
				the EOG.			
He, Ping, G.	ocular	adaptive	recursive	The non-	real	The	automatically
Wilson, and C.		filtering		stationary		approach does	•
Russell [30]			algorithm	component of		not scale up to	
				EOG signals is		situations with	
				monitored		four or more	without
				using this			sacrificing
				technique.		inputs.	performance

Chintala	r Robust	RVFF-RLS	The non-	Real and	Non-	The
. Chintala, ocula Sridhar, and artifa		based	The non- stationary	simulated	stationary	proposed
Jaisingh	Forgetting	algorithm	EOG signals			method
Thangaraj[32]	Factor (RVFF)		are followed			exhibits the
8Jt. 1	and Recursive		and estimated		tracking	lowest
	Least Square		by the		performance.	possible
	(RLS)		algorithm, and			mean square
			then the			error in a
			subtraction			time-varying
			approach is			condition.
			used to acquire clean EEG			
			clean EEG data.			
V. d	" EEMD 6-	Enganilata		D1	EEMD!»	D -44
Yadav, ocula Anchal, and artifa		Ensemble Empirical	To counter act EMD's		EEMD's amplitude-	Better constraints
Mahipal Singh	Kurtosis and		mode mixing		reduction	on ICA and
Choudhry. [33]	mMSE	Decomposition	U		problem	wavelet
enough [ee]			EEMD is		proorein	augmented
		Spatial	employed.			independent
		Constraint				component
		Independent				analysis can
		Component				boost
		Analysis				performance
		(SCICA)				even further.
Gajbhiye, ocula	r the FBSE-EWT	The	The approach	Real	The	Compared to
Pranjali, Rajeshartifa		Fourier-Bessel		Keai		existing
Kumar	separation	series	ocular artifact			methods, the
		1 1 1 1 1 1 1 1 1 1 1 1 1 1 1 1 1 1 1 1				,
Tripathy [34]	technique	expansion	from an EEG		various	proposed
Tripathy [34]	technique	expansion based empirical			various rhythmic EEG	proposed approach
Tripathy [34]	technique	based empirical wavelet	recording without the			approach improves
Tripathy [34]	technique	based empirical wavelet transform	recording without the use of a		rhythmic EEG	approach improves performance
Tripathy [34]	technique	based empirical wavelet	recording without the use of a reference		rhythmic EEG	approach improves performance while
Tripathy [34]	technique	based empirical wavelet transform	recording without the use of a		rhythmic EEG data appears	approach improves performance while requiring
Tripathy [34]	technique	based empirical wavelet transform	recording without the use of a reference		rhythmic EEG data appears	approach improves performance while requiring fewer
Tripathy [34]	technique	based empirical wavelet transform	recording without the use of a reference		rhythmic EEG data appears	approach improves performance while requiring fewer resources.
Tripathy [34]	technique	based empirical wavelet transform	recording without the use of a reference		rhythmic EEG data appears	approach improves performance while requiring fewer resources. When
Tripathy [34]	technique	based empirical wavelet transform	recording without the use of a reference		rhythmic EEG data appears	approach improves performance while requiring fewer resources. When compared to
Tripathy [34]	technique	based empirical wavelet transform	recording without the use of a reference		rhythmic EEG data appears	approach improves performance while requiring fewer resources. When
Tripathy [34]	technique	based empirical wavelet transform	recording without the use of a reference		rhythmic EEG data appears	approach improves performance while requiring fewer resources. When compared to other methods, alpha wave's
Tripathy [34]	technique	based empirical wavelet transform	recording without the use of a reference		rhythmic EEG data appears	approach improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD
Tripathy [34]	technique	based empirical wavelet transform	recording without the use of a reference		rhythmic EEG data appears	approach improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD value was
Tripathy [34]	technique	based empirical wavelet transform	recording without the use of a reference		rhythmic EEG data appears	approach improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD value was 0.029 on
		based empirical wavelet transform (FBSEEWT	recording without the use of a reference signal.		rhythmic EEG data appears	approach improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD value was 0.029 on average.
Islam, Md All ty	pe Entropy,	based empirical wavelet transform (FBSEEWT	recording without the use of a reference signal. The outcomes	Real &	rhythmic EEG data appears The	approach improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD value was 0.029 on average. The
Islam, Md All ty Kafiul, Parviz of	pe Entropy, kurtosis,	based empirical wavelet transform (FBSEEWT	recording without the use of a reference signal. The outcomes demonstrate	Real & simulated	rhythmic EEG data appears The proposed	approach improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD value was 0.029 on average. The proposed
Islam, Md All ty Kafiul, Parviz of Ghorbanzadeh, artifa	pe Entropy, kurtosis, cts skewness,	based empirical wavelet transform (FBSEEWT) stationary wavelet transform	recording without the use of a reference signal. The outcomes demonstrate that the		The proposed method still	approach improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD value was 0.029 on average. The proposed approach
Islam, Md All ty Kafiul, Parviz of Ghorbanzadeh, artifa and Amir remov	pe Entropy, kurtosis, cts skewness, val(periodic	stationary wavelet transform (FBSEEWT) stationary wavelet transform based artifact	recording without the use of a reference signal. The outcomes demonstrate		The proposed method still requires work	approach improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD value was 0.029 on average. The proposed approach utilizes four
Islam, Md All ty Kafiul, Parviz of Ghorbanzadeh, artifa	pe Entropy, kurtosis, cts skewness, val(periodic waveform index	stationary wavelet transform (FBSEEWT) stationary wavelet transform based artifact	recording without the use of a reference signal. The outcomes demonstrate that the suggested		The proposed method still	approach improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD value was 0.029 on average. The proposed approach utilizes four statistical
Islam, Md All ty Kafiul, Parviz of Ghorbanzadeh, artifa and Amirremo Rastegarnia. ECG,	rpe Entropy, kurtosis, cts skewness, val(periodic waveform index	stationary wavelet transform (FBSEEWT) stationary wavelet transform based artifact	recording without the use of a reference signal. The outcomes demonstrate that the suggested reduction of		The proposed method still requires work in terms of its	approach improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD value was 0.029 on average. The proposed approach utilizes four statistical techniques to
Islam, Md All ty Kafiul, Parviz of Ghorbanzadeh, artifa and Amirremo Rastegarnia. ECG, [35] EOG.	rpe Entropy, kurtosis, cts skewness, val(periodic waveform index	stationary wavelet transform (FBSEEWT) stationary wavelet transform based artifact	recording without the use of a reference signal. The outcomes demonstrate that the suggested reduction of artifacts		The proposed method still requires work in terms of its discrimination abilities and its capacity to	approach improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD value was 0.029 on average. The proposed approach utilizes four statistical techniques to plot the improbability
Islam, Md All ty Kafiul, Parvizof Ghorbanzadeh, artifa and Amirremo Rastegarnia. ECG, [35] EOG, EMG	rpe Entropy, kurtosis, cts skewness, val(periodic waveform index	stationary wavelet transform (FBSEEWT) stationary wavelet transform based artifact	recording without the use of a reference signal. The outcomes demonstrate that the suggested reduction of artifacts significantly		The proposed method still requires work in terms of its discrimination abilities and its	approach improves performance while requiring fewer resources. When compared to other methods, alpha wave's MAE in PSD value was 0.029 on average. The proposed approach utilizes four statistical techniques to plot the

Lag	Movemen	ICA with online	agnetrained	Examining the	Real &	Timeframes	Developed a
Lee,	t artifacts			_	simulated	for using the	-
Young-Eun,	tarmacis	learning	independent component	impact of noise	Simulated	approach are	rough estimate of
No-Sang				reduction in			
Kwak, and			•			constrained by	
Seong-Whan			online learning			the occurrence	
Lee [36]			(cIOL)	and frequency		of gait	artifacts
				domains		events. Anothe	
				through a			EEG data.
				quantitative			Finally,
				evaluation of		single adequate	
				artifact			EEG signals
				removal		represent	were
				approaches		artifacts' wide	recovered
				utilizing two		variety.	using
				BCI paradigms			weights that
				(ERP and			were updated
				SSVEP).			using online
							learning.
Song,	EMG	ICA, PCA, and	EMG-CCh	Reduce	simulate	Methodologica	Finally, the
YoungJae, and	artifacts	BSS-CCA		ambiguity and		1 Constraints	proposed
Francisco				enhance		An excessive	strategy
Sepulveda [37]				discrimination		amount of	improved
				between		class-	class
				classes.		dependent	separation
						EMG can	(when
							compared to
							prior
						reduced CRC	methods)
						during resting	using both
						conditions.	training and
							test data.
							The data set
							developed
							for the BCI
							competition
							is used in a
							wide variety
							of
							applications.
							This strategy
							can be used
							independentl
							y or in
							tandem with
							other
							approaches
							of managing
							artifacts.

According to the data in the table above, the most common techniques used to clean up EEG signals include Blind Source Separation (BSS), Principal Component Analysis (PCA), Canonical Correlation Analysis (CCA), Discrete Wavelet Transform (DWT), Stationary Wavelet Transform (SWT), Empirical Mode Decomposition (EMD), Ensemble Empirical Mode Decomposition (EEMD), Wavelet Transform, and Adaptive Filtering. The performance parameters,

including the correlation co-efficient, Mean Square Error, Power Spectral Density, Signal-to-Noise Ratio, and Execution Speed and Complexity, are all improved when the preprocessing stage is enhanced.

The above table details a discussion of advanced artifact removal techniques for the examples given, including those by nar, Salim(2021), who discussed and implemented a new algorithm, the classical Least Mean Squares (LMS) algorithm, and the Normalized LMS algorithm (using Independent Component Analysis, Kurtosis, K-means, a modified Z-score, and an adaptive noise canceler) for removing eye blink artifacts from both real and simulated data. The system has the limitation of only being able to deal with ocular artifacts, making it a less-than-efficient method; the subtraction process can result in the loss of important EEG signals; and in another paper by Borowicz and Adam, they discussed independent component analysis (ICA) and regression analysis principles and implemented them using a multichannel Wiener filter; and in this study, they used a subset of frontal electrodes to detect ICA. It also works great with real-time systems, which is apparently crucial for BCI research. Additionally, a novel concept was implemented by Zhou, Weidong, and Jean Gotman using Independent Component Analysis in combination with the EEG dipole model, with a primary focus on ocular artifact elimination. This technique was found to be effective in automatically eradicating ocular artifacts from the EEG. Song, YoungJae, and Francisco Sepulveda also implemented the system using ICA, in addition to PCA, and BSS-CCA to remove EMG artifacts by a novel technique called EMG-cch and best suited for use along with the other techniques the data only implemented on simulation results.

Genetic algorithm (GA), a technique proposed by Trigui, Omar, et al., decreases the RMSE between unprocessed and processed EEG data. Using only simulated data and a small number of channels, the proposed approach nevertheless achieves satisfactory results.

Each and every eye blink artifact was correctly identified by the proposed method by Cao, Jiuwen.etal, with zero false positives.

The method developed by Egambaram, Ashvaany, et al. CFast EMD-CCA and Fast CCA introduced a method for detecting eye blink artifacts without human supervision by combining a variant of Empirical Mode Decomposition with Canonical Correlation Analysis. Artifact-free EEG segments showed hardly any distortion, with an accuracy of more than 97% and a removal speed of 10-13 ms, on average. Artifacts caused by an eyeblink can be corrected online with minimal neural distortion.

To eliminate EB artifacts from the EEG signal, Sreeja, S. R., et al. suggested a method known as K-SVD with morphological component analysis. Both of these methods are sparsity-based methodologies that work on both real and simulated data without the need for channel information, parameter tweaking (such as thresholding), or additional hardware/EEG channels.

Adaptive filtering for ocular artifacts using recursive least squares was given by He, Ping, G. Wilson, and C. Russell. When applied to real-world data, this method follows the dynamic components of EOG signals. It cannot be generalized to situations involving three or more reference inputs, but it can be automatically adapted to a new setting without compromising its efficacy.

Using the Robust Variable Forgetting Factor (RVFF) and Recursive Least Square (RLS), Chintala, Sridhar, and Jaisingh Thangaraj solved the problem of ocular artifacts. This method estimates and follows non-stationary EOG signals so that pure EEG signals can be extracted from both real and simulated data. In unstable conditions, tracking accuracy decreases. The proposed method achieves the smallest mean square error in a dynamic environment.

Yadav, Anchal, and Mahipal Singh Choudhry compute Kurtosis and mean squared error (mSSE) using Ensemble Empirical Mode Decomposition (EEMD) and Spatial Constraint Independent Component Analysis (SCICA). EEMD is also used to overcome the mode mixing and aliasing problem of EMD, which is typically performed on Real data. Improving the constraints used in ICA and wavelet-enhanced independent component analysis can further boost performance. In order to get rid of ocular artifacts, Gajbhiye, Pranjali, and Rajesh Kumar Tripathy presented a rhythm separation technique based on FBSE-EWT. Ocular artifacts can be removed from an EEG signal using the Fourier-Bessel series expansion based empirical wavelet transform (FBSEEWT) method, which has been extensively validated for real-valued data and does not require a reference signal. When many modes of EEG rhythm information appear, this phenomenon is referred to as "mode mixing." The suggested method outperforms state-of-the-art alternatives, with a mean absolute error (MAE) in peak signal-to-noise ratio (PSR) of only 0.029 for rhythm.

Using entropy, kurtosis, skewness, and the stationary wavelet transform, Islam, Md. Kafiul, Parviz Ghorbanzadeh, and Amir Rastegarnia proposed a method for eliminating artifacts across all modalities. When evaluated with real and simulated data, the results reveal that the proposed artefact removal significantly improves BCI output. The proposed technique still needs better discrimination capacity and has weak ability to eliminate genuine artefacts. The suggested method for mapping artificial probability uses four statistical parameters.

3. CONCLUSION

The work is mostly considered in the preprocessing step of the overall BCI systems. The goal of the pre-processing

stage in a BCI applications is to decrease artifacts in the EEG signal generated by the numerous sources. Based on the findings in the available literature, this report summarized the key techniques, Some of the techniques uses exclusively used for removing artifacts which is related to eye blink (EOG)artifacts, ECG ,EMG and all other movement related artifacts here by go through the different research articles basically uses different algorithams separately or combinely that reveals the output without artifacts in EEG signal processing which combined with BCI related applications either it may be cursor movement, wheel chair movement, video gaming, bio medical etc. Some methods, such as adaptive filtering, Morphological Component Analysis (MCA) and K-SVD and Entropy, kurtosis, skewness, periodic waveform index, remove artifacts with high precision, which works on both real and simulated data or either of the one, however methods with high computational cost may not be suited for online applications. As a result, there is no best option for removing all forms of artifacts. So, one of the future goals of effective artifact attenuation is to provide an application-specific methodology with improved time and precision, efficiency.

Data Availability. Data underlying the results presented in this paper are available from the corresponding author upon reasonable request.

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Ethics. The authors declare that the present research work has fulfilled all relevant ethical guidelines required by COPE.



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REFERENCES

- [1] Kübler, A. (2020). The history of BCI: From a vision for the future to real support for personhood in people with locked-in syndrome. *Neuroethics*, *13*(2), 163-180.
- [2] Kawala-Janik, A. Efficiency Evaluation of External Environments Control Using Bio-Signals. Ph.D. Thesis, University of Greenwich, London, UK, 2013.
- [3] Ebersole, J.S.; Pedley, T.A. Current Practice of Clinical Electroencephalography; Lippincott Williams & Wilkins: Philadelphia, PA, USA, 2003
- [4] Millett, D. Hans Berger: From psychic energy to the EEG. Perspect. Biol. Med. 2001, 44, 522–542. [CrossRef] Priyanka A. Abhang, Bharti W. Gawali, Suresh C. Mehrotra,
- [5] Chapter 2 Technological Basics of EEG Recording and Operation of Apparatus, Editor(s): Priyanka A. Abhang, Bharti W. Gawali, Suresh C. Mehrotra, Introduction to EEG- and Speech-Based Emotion Recognition, Academic Press, 2016
- [6] Aggarwal, Swati, and Nupur Chugh. "Signal processing techniques for motor imagery brain computer interface: A review," Array 1 (2019): 100003.
- [7] Donoghue JP. Connecting cortex to machines: recent advances in brain interfaces. Nat Neurosci 2002;5:1085.
- [8] 8.Serruya Mijail D, et al. Brain-machine interface: instant neural control of a movement signal. Nature 2002;416:141.
- [9] Cichocki, Andrzej, et al. "EEG filtering based on blind source separation (BSS) for early detection of Alzheimer's disease." Clinical Neurophysiology 116.3 (2005): 729-737.
- [10] Al-Fahoum, Amjed S., and Ausilah A. Al-Fraihat. "Methods of EEG signal features extraction using linear analysis in frequency and time-frequency domains." International Scholarly Research Notices 2014 (2014).
- [11] Osalusi, Bamidele, Amole Abraham, and David Aborisade. "EEG Classification in Brain Computer Interface (BCI): A Pragmatic Appraisal." *American Journal of Biomedical Engineering* 8.1 (2018): 1-11.
- [12] Mridha, M. F., et al. "Brain-computer interface: Advancement and challenges." Sensors 21.17 (2021): 5746.
- [13] Phan A H and Cichocki A 2010 Tensor decompositions for feature extraction and classification of high dimensional datasets Nonlinear Theory Appl. 1 37–68
- [14] Washizawa Y, Higashi H, Rutkowski T, Tanaka T and Cichocki A 2010 Tensor based simultaneous feature extraction and sample weighting for EEG classification Int. Conf. on Neural Information Processing, ICONIP 2010: Neural Information Processing. Models and Applications (Berlin: Springer) pp 26–33
- [15] Onishi A, Phan A, Matsuoka K and Cichocki A 2012 Tensor classification for P300-based brain computer interface IEEE Int. Conf. on Acoustics, Speech and Signal Processing (IEEE) pp 581–4
- [16] Zhang Y, Zhou G, Jin J, Wang X and Cichocki A 2014, "Frequency recognition in SSVEP-based BCI using multiset canonical correlation analysis". Int. J. Neural Syst. 24 1450013
- [17] Zhang Y, Zhou G, Jin J, Wang X and Cichocki A 2015 Optimizing spatial patterns with sparse filter bands for motor-imagery based brain—computer interface J. Neurosci. Methods 255 85–91

- [18] Zhang, Y. U., Zhou, G., Jin, J., Wang, X., & Cichocki, A. (2014). "Frequency recognition in SSVEP-based BCI using multiset canonical correlation analysis". *International journal of neural systems*, 24(04), 1450013.
- [19] Zhang, Y., Zhou, G., Jin, J., Wang, X., & Cichocki, A. (2015). "Optimizing spatial patterns with sparse filter bands for motor-imagery based brain-computer interface". *Journal of neuroscience methods*, 255, 85-91.
- [20] Zhang, Y., Zhou, G., Jin, J., Zhang, Y., Wang, X., & Cichocki, A. (2017). "Sparse Bayesian multiway canonical correlation analysis for EEG pattern recognition". *Neurocomputing*, 225, 103-110.
- [21] Zhang Y, Zhou G, Zhao Q, Onishi A, Jin J, Wang Xand Cichocki, 2011, "Multiway canonical correlationanalysis for frequency components recognition in SSVEP-based BCIs", Neural Information Processing (Berlin: Springer)
- [22] Çınar, Salim. "Design of an automatic hybrid system for removal of eye-blink artifacts from EEG recordings." Biomedical Signal Processing and Control 67 (2021): 102543.
- [23] Trigui, Omar, et al. "Removal of eye blink artifacts from EEG signal using morphological modeling and orthogonal projection." Signal, Image and Video Processing 16.1 (2022): 19-27.
- [24] Cao, Jiuwen, et al. "Unsupervised eye blink artifact detection from EEG with Gaussian mixture model." *IEEE Journal of Biomedical and Health Informatics* 25.8 (2021): 2895-2905.
- [25] Wang, Jianhui, et al. "Eye blink artifact detection with novel optimized multi-dimensional electroencephalogram features." IEEE Transactions on Neural Systems and Rehabilitation Engineering 29 (2021): 1494-1503.
- [26] Egambaram, Ashvaany, et al. "Online detection and removal of eye blink artifacts from electroencephalogram." Biomedical Signal Processing and Control 69 (2021): 102887.
- [27] Borowicz, Adam. "Using a multichannel Wiener filter to remove eye-blink artifacts from EEG data." Biomedical Signal Processing and Control 45 (2018): 246-255.
- [28] Zhou, Weidong, and Jean Gotman. "Automatic removal of eye movement artifacts from the EEG using ICA and the dipole model." *Progress in Natural Science* 19.9 (2009): 1165-1170.
- [29] Sreeja, S. R., et al. "Removal of eye blink artifacts from EEG signals using sparsity." *IEEE journal of biomedical and health informatics* 22.5 (2017): 1362-1372.
- [30] He, Ping, G. Wilson, and C. Russell. "Removal of ocular artifacts from electro-encephalogram by adaptive filtering." *Medical and biological engineering and computing* 42.3 (2004): 407-412.
- [31] Joyce, Carrie A., Irina F. Gorodnitsky, and Marta Kutas. "Automatic removal of eye movement and blink artifacts from EEG data using blind component separation." *Psychophysiology* 41.2 (2004): 313-325.
- [32] Chintala, Sridhar, and Jaisingh Thangaraj. "Ocular artifact elimination from eeg signals using rvff-rls adaptive algorithm." 2020 National Conference on Communications (NCC). IEEE, 2020.
- [33] Yadav, Anchal, and Mahipal Singh Choudhry. "A new approach for ocular artifact removal from EEG signal using EEMD and SCICA." Cogent Engineering 7.1 (2020): 1835146.
- [34] Gajbhiye, Pranjali, Rajesh Kumar Tripathy, and Ram Bilas Pachori. "Elimination of ocular artifacts from single channel EEG signals using FBSE-EWT based rhythms." *IEEE Sensors Journal* 20.7 (2019): 3687-3696.
- [35] Islam, Md Kafiul, Parviz Ghorbanzadeh, and Amir Rastegarnia. "Probability mapping based artifact detection and removal from single-channel EEG signals for brain-computer interface applications." Journal of Neuroscience Methods 360 (2021): 109249.
- [36] Lee, Young-Eun, No-Sang Kwak, and Seong-Whan Lee. "A real-time movement artifact removal method for ambulatory brain-computer interfaces." IEEE Transactions on Neural Systems and Rehabilitation Engineering 28.12 (2020): 2660-2670.
- [37] Song, Y., & Sepulveda, F. (2018). "A novel technique for selecting EMG-contaminated EEG channels in self-paced brain-computer Interface task onset". IEEE Transactions on neural systems and rehabilitation engineering, 26(7), 1353-1362.
- [38] Krauledat, Matthias, et al. "Robustifying EEG data analysis by removing outliers." Chaos and Complexity Letters 2.3 (2007): 259-274. J. Clerk Maxwell, A Treatise on Electricity and Magnetism, 3rd ed., vol. 2. Oxford: Clarendon, 1892, pp.68–73.
- [39] Gouy-Pailler, Cédric, et al. "Iterative subspace decomposition for ocular artifact removal from EEG recordings." International Conference on Independent Component Analysis and Signal Separation. Springer, Berlin, Heidelberg, 2009. K. Elissa, "Title of paper if known," unpublished.
- [40] Croft, Rodney J., et al. "EOG correction: a comparison of four methods." Psychophysiology 42.1 (2005): 16-24. Y. Yorozu, M. Hirano, K. Oka, and Y. Tagawa, "Electron spectroscopy studies on magneto-optical media and plastic substrate interface," IEEE Transl. J. Magn. Japan, vol. 2, pp. 740–741, August 1987 [Digests 9th Annual Conf. Magnetics Japan, p. 301, 1982].
- [41] M. Young, The Technical Writer's Handbook. Mill Valley, CA: University Science, 1989.
- [42] Jiang, Aimin, et al. "Efficient CSP algorithm with spatio-temporal filtering for motor imagery classification." IEEE Transactions on Neural Systems and Rehabilitation Engineering 28.4 (2020): 1006-1016.
- [43] Isa, NE Md, et al. "Motor imagery classification in Brain computer interface (BCI) based on EEG signal by using machine learning technique." Bulletin of Electrical Engineering and Informatics 8.1 (2019): 269-275.
- [44] Ang, Kai Keng, et al. "Filter bank common spatial pattern (FBCSP) in brain-computer interface." 2008 IEEE international joint conference on neural networks (IEEE world congress on computational intelligence). IEEE, 2008.
- [45] Ramoser, Herbert, Johannes Muller-Gerking, and Gert Pfurtscheller. "Optimal spatial filtering of single trial EEG during imagined hand movement." *IEEE transactions on rehabilitation engineering* 8.4 (2000): 441-446.

- [46] Oh, Seung-Hyeon, Yu-Ri Lee, and Hyoung-Nam Kim. "A novel EEG feature extraction method using Hjorth parameter." International Journal of Electronics and Electrical Engineering 2.2 (2014): 106-110.
- [47] Übeyli, Elif Derya, and İnan Güler. "Features extracted by eigenvector methods for detecting variability of EEG signals." Pattern Recognition Letters 28.5 (2007): 592-603.
- [48] Stancin, Igor, Mario Cifrek, and Alan Jovic. "A review of EEG signal features and their application in driver drowsiness detection systems." Sensors 21.11 (2021): 3786.
- [49] Stam, CJ van, and E. C. W. Van Straaten. "The organization of physiological brain networks." Clinical neurophysiology 123.6 (2012): 1067-1087.
- [50] Übeyli, Elif Derya. "Analysis of EEG signals by implementing eigenvector methods/recurrent neural networks." Digital Signal Processing 19.1 (2009): 134-143.
- [51] Gaur, Pramod, et al. "A sliding window common spatial pattern for enhancing motor imagery classification in EEG-BCI." *IEEE Transactions on Instrumentation and Measurement* 70 (2021): 1-9.
- [52] Bose, Rohit, et al. "Performance analysis of left and right lower limb movement classification from EEG." 2016 3rd International Conference on Signal Processing and Integrated Networks (SPIN). IEEE, 2016.
- [53] Raschka, Sebastian, David Julian, and John Hearty. Python: deeper insights into machine learning. Packt Publishing Ltd, 2016.
- [54] Isa, NE Md, et al. "Motor imagery classification in Brain computer interface (BCI) based on EEG signal by using machine learning technique." Bulletin of Electrical Engineering and Informatics 8.1 (2019): 269-275.
- [55] Rish, Irina. "An empirical study of the naive Bayes classifier." IJCAI 2001 workshop on empirical methods in artificial intelligence. Vol. 3. No. 22. 2001.
- [56] Leung, K. Ming. "Naive bayesian classifier." Polytechnic University Department of Computer Science/Finance and Risk Engineering 2007 (2007): 123-156.
- [57] Berrar, Daniel. "Cross-Validation." (2019): 542-545.
- [58] Ang, Kai Keng, et al. "Filter bank common spatial pattern algorithm on BCI competition IV datasets 2a and 2b." Frontiers in neuroscience 6 (2012): 39.
- [59] Shenoy, H. Vikram, A. Prasad Vinod, and Cuntai Guan. "Shrinkage estimator based regularization for EEG motor imagery classification." 2015 10th International Conference on Information, Communications and Signal Processing (ICICS). IEEE, 2015.
- [60] Lupu, R. G., Ungureanu, F., & Cimpanu, C. (2019, May). "Brain-computer interface: Challenges and research perspectives". In 2019 22nd International Conference on Control Systems and Computer Science (CSCS) (pp. 387-394). IEEE.
- [61] Fouad, M. M., Amin, K. M., El-Bendary, N., & Hassanien, A. E. (2015). "Brain computer interface: a review". Brain-computer interfaces, 3-30.
- [62] Urigüen, J. A., & Garcia-Zapirain, B. (2015). "EEG artifact removal—state-of-the-art and guidelines". Journal of neural engineering, 12(3), 031001.
- [63] Islam, M. K., Rastegarnia, A., & Yang, Z. (2016). "Methods for artifact detection and removal from scalp EEG: A review". Neurophysiologie Clinique/Clinical Neurophysiology, 46(4-5), 287-305.
- [64] Mumtaz, W., Rasheed, S., & Irfan, A. (2021). "Review of challenges associated with the EEG artifact removal methods". Biomedical Signal Processing and Control. 68, 102741.
- [65] Radüntz, T., Scouten, J., Hochmuth, O., & Meffert, B. (2015). "EEG artifact elimination by extraction of ICA-component features using image processing algorithms". *Journal of neuroscience methods*, 243, 84-93.
- [66] Radüntz, T., Scouten, J., Hochmuth, O., & Meffert, B. (2017). "Automated EEG artifact elimination by applying machine learning algorithms to ICA-based features". *Journal of neural engineering*, 14(4), 046004.
- [67] Roy, V., Shukla, P. K., Gupta, A. K., Goel, V., Shukla, P. K., & Shukla, S. (2021). "Taxonomy on EEG artifacts removal methods, issues, and healthcare applications". *Journal of Organizational and End User Computing (JOEUC)*, 33(1), 19-46
- [68] Mannan, M. M. N., Kamran, M. A., & Jeong, M. Y. (2018). "Identification and removal of physiological artifacts from electroencephalogram signals: A review". *Ieee Access*, 6, 30630-30652.
- [69] Gevins, A. S., Yeager, C. L., Zeitlin, G. M., Ancoli, S., & Dedon, M. F. (1977). "On-line computer rejection of EEG artifact". Electroencephalography and clinical Neurophysiology, 42(2), 267-274.
- [70] Park, H. J., Jeong, D. U., & Park, K. S. (2002). "Automated detection and elimination of periodic ECG artifacts in EEG using the energy interval histogram method". *IEEE transactions on Biomedical Engineering*, 49(12), 1526-1533.
- [71] Nolan, H., Whelan, R., & Reilly, R. B. (2010). "FASTER: fully automated statistical thresholding for EEG artifact rejection". Journal of neuroscience methods, 192(1), 152-162.
- [72] Tatum, W. O., Dworetzky, B. A., & Schomer, D. L. (2011). "Artifact and recording concepts in EEG". *Journal of clinical neurophysiology*, 28(3), 252-263.
- [73] Jung, C. Y., & Saikiran, S. S. (2016). "A review on EEG artifacts and its different removal technique". Asia-pacific Journal of Convergent Research Interchange, 2(4), 43-60.
- [74] Jiang, X., Bian, G. B., & Tian, Z. (2019). "Removal of artifacts from EEG signals: a review". Sensors, 19(5), 987.
- [75] Rohál'ová, M., Sykacek, P., Koskaand, M., & Dorffner, G. (2001). "Detection of the EEG Artifacts by the Means of the (Extended) Kalman Filter". Meas. Sci. Rev, 1(1), 59-62.
- [76] Blum, S., Jacobsen, N. S., Bleichner, M. G., & Debener, S. (2019). "A Riemannian modification of artifact subspace reconstruction for EEG artifact handling". Frontiers in human neuroscience, 13, 141.

- [77] Shao, S. Y., Shen, K. Q., Ong, C. J., & Wilder-Smith, E. P. (2008). "Automatic EEG artifact removal: a weighted support vector machine approach with error correction". *IEEE Transactions on Biomedical Engineering*, 56(2), 336-344.
- [78] Nejedly, P., Cimbalnik, J., Klimes, P., Plesinger, F., Halamek, J., Kremen, V., ... & Jurak, P. (2019). "Intracerebral EEG artifact identification using convolutional neural networks". Neuroinformatics, 17(2), 225-234.
- [79] Somers, B., Francart, T., & Bertrand, A. (2018). "A generic EEG artifact removal algorithm based on the multi-channel Wiener filter". *Journal of neural engineering*, 15(3), 036007.
- [80] Saba-Sadiya, S., Chantland, E., Alhanai, T., Liu, T., & Ghassemi, M. M. (2021). "Unsupervised EEG artifact detection and correction". Frontiers in digital health, 2, 608920.
- [81] Islam, M. K., Rastegarnia, A., & Yang, Z. (2016). "Methods for artifact detection and removal from scalp EEG: A review". Neurophysiologie Clinique/Clinical Neurophysiology, 46(4-5), 287-305.
- [82] Abreu, R., Leal, A., & Figueiredo, P. (2018). "EEG-informed fMRI: a review of data analysis methods". Frontiers in human neuroscience, 12, 29.
- [83] Varone, G., Hussain, Z., Sheikh, Z., Howard, A., Boulila, W., Mahmud, M., ... & Hussain, A. (2021). "Real-time artifacts reduction during TMS-EEG co-registration: a comprehensive review on technologies and procedures". Sensors, 21(2), 637.
- [84] Jung, T. P., Humphries, C., Lee, T. W., Makeig, S., McKeown, M. J., Iragui, V., & Sejnowski, T. J. (1998, September).
 "Removing electroencephalographic artifacts: comparison between ICA and PCA". In Neural Networks for Signal Processing VIII. Proceedings of the 1998 IEEE Signal Processing Society Workshop (Cat. No. 98TH8378) (pp. 63-72). IEEE.
- [85] Anderer, P., Roberts, S., Schlögl, A., Gruber, G., Klösch, G., Herrmann, W., ... & Saletu, B. (1999). "Artifact processing in computerized analysis of sleep EEG-a review". *Neuropsychobiology*, 40(3), 150-157.
- [86] Chen, X., Xu, X., Liu, A., Lee, S., Chen, X., Zhang, X., ... & Wang, Z. J. (2019). "Removal of muscle artifacts from the EEG: a review and recommendations". *IEEE Sensors Journal*, 19(14), 5353-5368.
- [87] Cao, K., Guo, Y., & Su, S. W. (2015, December). "A review of motion related EEG artifact removal techniques". In 2015 9th International Conference on Sensing Technology (ICST) (pp. 600-604). IEEE.
- [88] Klekowicz, H., Malinowska, U., Piotrowska, A. J., Wołyńczyk-Gmaj, D., Niemcewicz, S., & Durka, P. J. (2009). "On the robust parametric detection of EEG artifacts in polysomnographic recordings". *Neuroinformatics*, 7(2), 147-160.
- [89] Minguillon, J., Lopez-Gordo, M. A., & Pelayo, F. (2017). "Trends in EEG-BCI for daily-life: Requirements for artifact removal". Biomedical Signal Processing and Control, 31, 407-418.
- [90] Sadiya, S., Alhanai, T., & Ghassemi, M. M. (2021, May). "Artifact detection and correction in eeg data: A review". In 2021 10th International IEEE/EMBS Conference on Neural Engineering (NER) (pp. 495-498). IEEE.
- [91] Craik, A., He, Y., & Contreras-Vidal, J. L. (2019). "Deep learning for electroencephalogram (EEG) classification tasks: a review". *Journal of neural engineering*, 16(3), 031001.
- [92] Haumann, N. T., Parkkonen, L., Kliuchko, M., Vuust, P., & Brattico, E. (2016). "Comparing the performance of popular MEG/EEG artifact correction methods in an evoked-response study". Computational Intelligence and Neuroscience, 2016.
- [93] Sazgar, M., & Young, M. G. (2019). "EEG artifacts". Absolute epilepsy and EEG rotation review (pp. 149-162). Springer, Cham.
- [94] Jung, T. P., Makeig, S., Humphries, C., Lee, T. W., Mckeown, M. J., Iragui, V., & Sejnowski, T. J. (2000). "Removing electroencephalographic artifacts by blind source separation". *Psychophysiology*, 37(2), 163-178.
- [95] Kaya, I. (2019). "A brief summary of EEG artifact handling". Brain-Computer Interface.
- [96] Taherisadr, M., Dehzangi, O., & Parsaei, H. (2017). "Single channel EEG artifact identification using two-dimensional multi-resolution analysis". Sensors, 17(12), 2895.
- [97] Jafarifarmand, A., & Badamchizadeh, M. A. (2019). "EEG artifacts handling in a real practical brain-computer interface controlled vehicle". *IEEE Transactions on Neural Systems and Rehabilitation Engineering*, 27(6), 1200-1208.
- [98] Gorjan, D., Gramann, K., De Pauw, K., & Marusic, U. (2022). "Removal of movement-induced EEG artifacts: current state of the art and guidelines". *Journal of neural engineering*.
- [99] Hartmann, M. M., Schindler, K., Gebbink, T. A., Gritsch, G., & Kluge, T. (2014). "PureEEG: Automatic EEG artifact removal for epilepsy monitoring". Neurophysiologie Clinique/Clinical Neurophysiology, 44(5), 479-490.
- [100] Muthukumaraswamy, S. D. (2013). "High-frequency brain activity and muscle artifacts in MEG/EEG: a review and recommendations". Frontiers in human neuroscience, 7, 138.
- [101] Kang, G., Jin, S. H., Kim, D. K., & Kang, S. W. (2018). T59. "EEG artifacts removal using machine learning algorithms and independent component analysis". Clinical Neurophysiology, 129, e24.